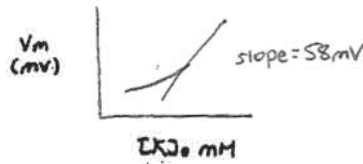


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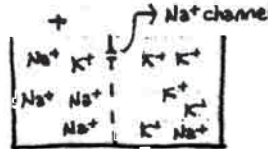
$E_K \sim V_r$ (not exactly, but close enough)

- change molar concentration on outside, see if E_K changes in predictable fashion
- changing $[K^+]_o$ by factor of 10 changes E_K by 58 mV
- however, at lower values of $[K^+]_o$, something else happens



to determine resting potential, need to take into account E_{Na} as well as E_K

- 99 K^+ holes for each 1 Na^+ hole
- error on terms of $\sim 10\%$
- (high $[Na^+]_o$ trying to get through, few channels to go through)



Nernst equation: $V_m = 58 \text{ mV} \log \frac{[K^+]_i}{[K^+]_o + \frac{P_{Na}/P_K [Na^+]_o + P_{Cl}/P_K [Cl^-]_o}{[K^+]_i}}$

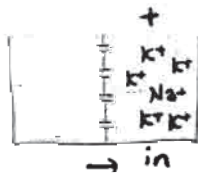
permeability (weights concentrations): measure w/ radioactive K^+ or Na^+ , look at rate of diffusion

becomes Goldman equation (at high negative V_r s, predicts V_r)

$[Na^+]_o$ so much higher than $[K^+]_o$ that adds appreciable current drive at lower $[K^+]_o$.

- resting potential from gradients + ion-selective channels + pumps

if Na^+ -permeable membrane only



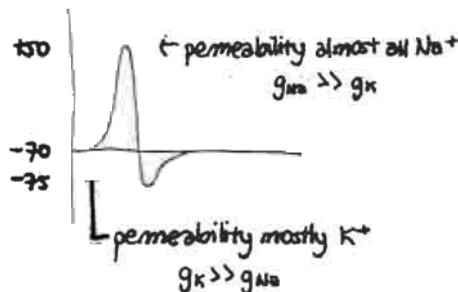
cell would be inside positive

$$V = 58 \text{ mV} \log \frac{[Na^+]_o}{[Na^+]_i}$$

$\sim 58 \text{ mV}$ (pos. inside)

similar to top of action potential

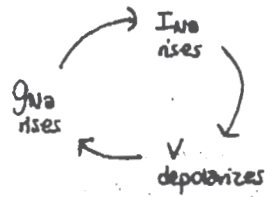
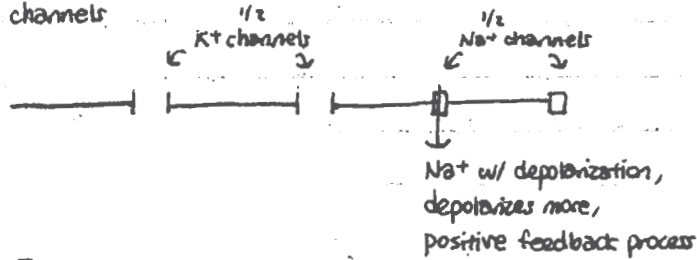
- action potential switches membrane conductance to ions



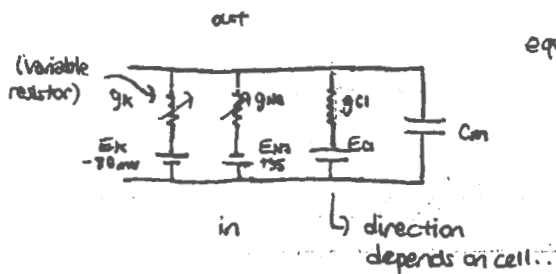
change outside concentration of Na^+ : removing $1/2 Na^+$ + replacing w/ impermeant ion decreases maximum of action potential

- switching of ion channel conductances based on threshold voltage (-58 mV)

- these are voltage-gated channels



positive feedback cycle
(explains threshold)



equivalent circuit for membrane

pumps give you gradients (pumps not batteries)
voltage from gradient is battery

Ohm's Law for membranes -

$$I = \frac{V}{R} = V/R$$

inward flow of positive ions → negative current
(textbook uses this convention, Hodgkin/Huxley use other)

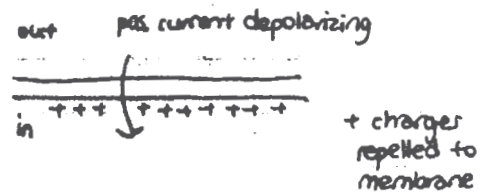
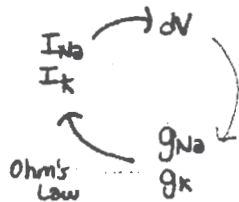
$$I = gV$$

$$I = I_K + I_{Na}$$

$$= g_K \left(\frac{V_m - E_K}{E_K - V_m} \right) + g_{Na} (V_m - E_{Na})$$

(Ohm's law for individual membrane currents)

when $V_m = 0$, g_K not 0, so must be
proportional to where V_m is and where
 E_K wants it to be



know I, know $\Delta V \left(\frac{dV}{dt} \right)$

current/
all charges come in to charge, dist discharge C_m
1 mol electrons must be compensated

$Q = CV$ (definition of capacitance)

(voltage across plates \times voltage)

$$\frac{dQ}{dt} = \frac{dV}{dt} (C) \times V \frac{dC}{dt}$$

\hookrightarrow no $\frac{dC}{dt}$

$$I = C \frac{dV}{dt}$$

all lipid bilayer membranes have \sim same capacitance

$$= 1 \mu F / cm^2$$

$$m\Omega \times 1 \mu F = 1 s \quad (\text{for RC time constants})$$

if you know I and C ,

know new voltage

- can reconstruct action potential

(measure g_{Na} , g_K)

\hookrightarrow see how g_{Na} , g_K vary w/ voltage

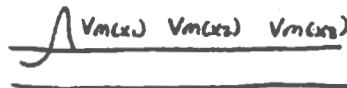
measuring these is holy grail



Hodgkin + Huxley experiments:

- measure g_K , g_{Na}

- but in unconstrained axon, $V_m(x_1)$, $V_m(x_2)$, $V_m(x_3)$ all different



each patch at different voltage, also influencing each other (current flow between them)

problems:

1. spatial variation in V_m
2. temporal variation in V_m
3. how to separate I_K , I_{Na} ?

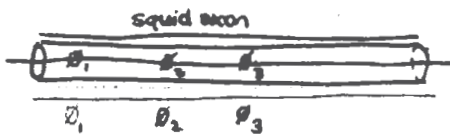
even in individual patch, patch, V_m will change (can't measure g as fx of V_m)

(don't know details)

will get Na^+ and K^+ currents: how to differentiate?
will only get one electrically measured current

1. H + H eliminated spatial variation in V_m by putting wire inside axon, close ones outside: short circuits changes in potential

Space clamp



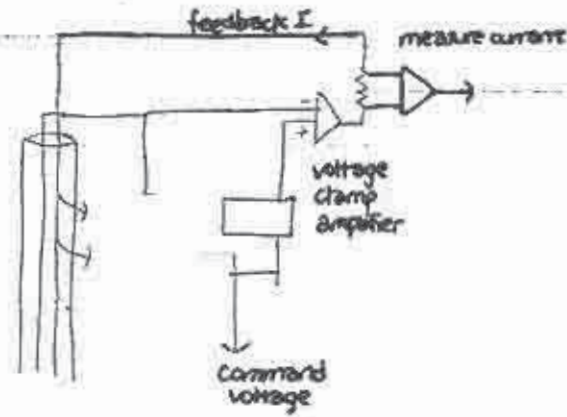
all salt water outside close to membrane will also be at same potential

all inside will be at one potential b/c wire is good conductor, current will flow to eliminate voltage (Ohm's Law w/ hardly any R)

no electric field inside conductor

2. H + H used electronics to artificially damp V_m where they wanted it

- inject currents I_n to keep V_m at one value (small values of μA s, nAe)



inject positive current if inside negative
will settle down if no input to amplifier

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